

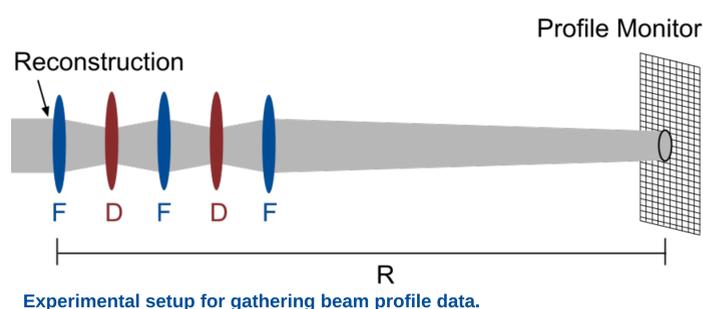
Computed Tomography of Transverse Phase Space

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Beam Tomography

The transverse phase space distribution of a particle beam can be reconstructed from profile information with the same computed tomography algorithms used in the medical industry.

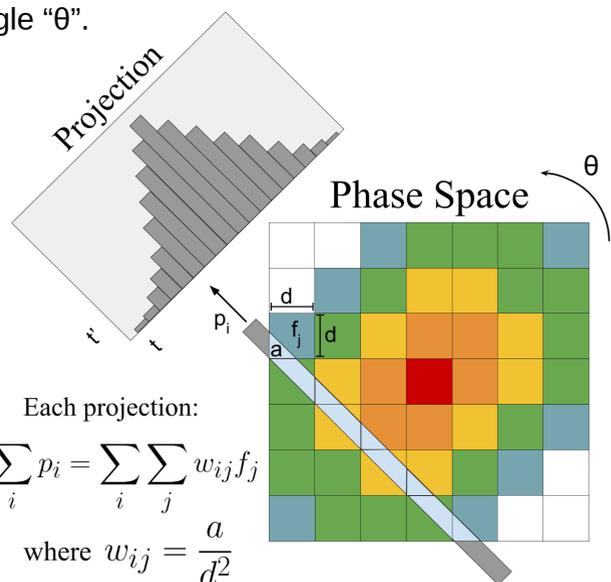
Beam profiles are taken at a single point in a beamline while varying the optics between the profile monitor and the reconstruction location.



For linear transfer matrix R between the point of reconstruction and the profile monitor, we define the scaling factor “ s ” and phase space orientation angle “ θ ” as:

$$s = \sqrt{R_{11}^2 + R_{12}^2} \quad \theta = \tan^{-1}\left(\frac{R_{12}}{R_{11}}\right)$$

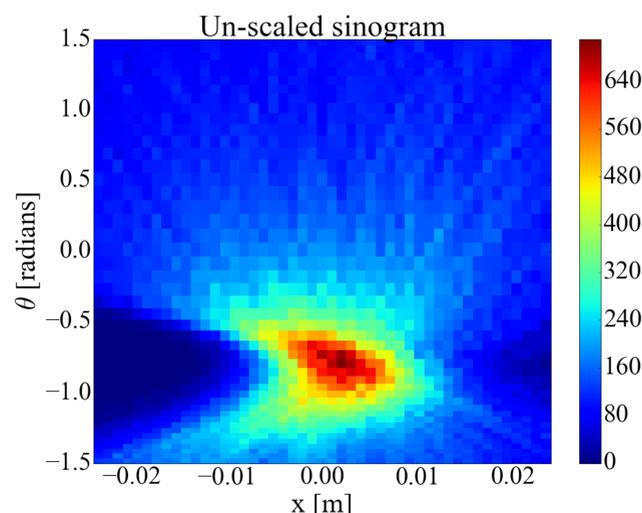
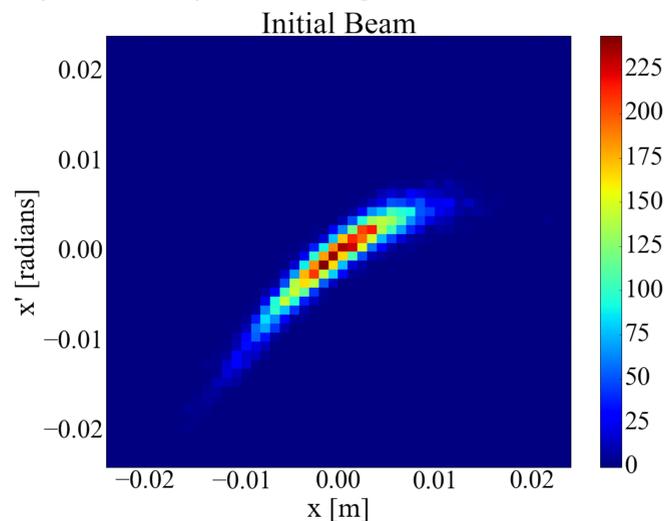
Scaling each beam profile horizontally by “ $1/s$ ” and vertically by “ s ” lets us consider each profile as a one-dimensional projection of the two-dimensional phase space for that plane. Each projection is a “view” of the phase space through angle “ θ ”.



Each scaled beam profile is a one-dimensional projection of the two-dimensional phase space.

Beam Simulation

A deliberately non-elliptical and asymmetric beam distribution is created as a list of particle (x, x') vectors, then passed one-by-one through a symmetric FODO channel using the thick-lens linear transfer matrices. Fixed-bin histograms simulate multiwire profile data for each beamline tune. Each row of the resulting “sinogram” represents a profile at angle “ θ ”.



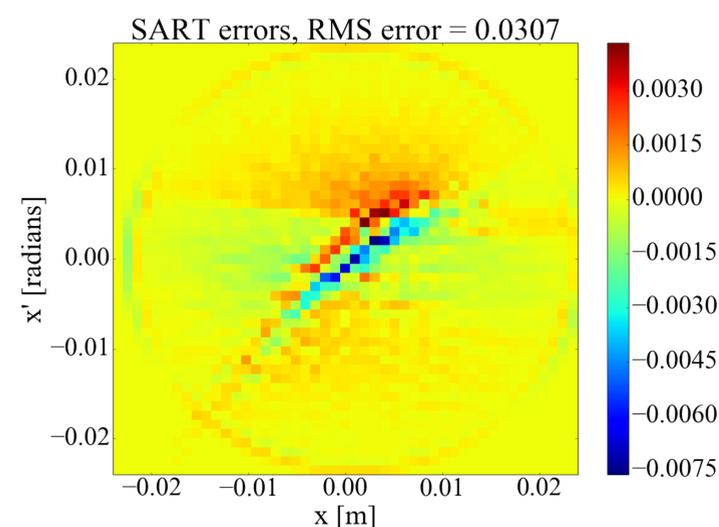
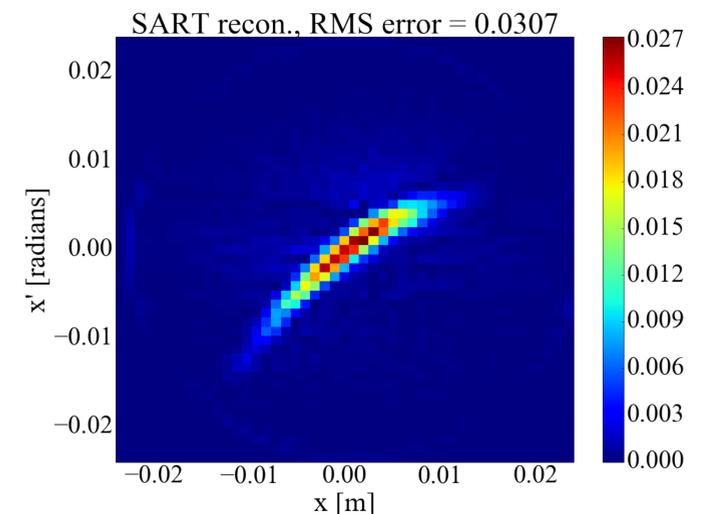
Initial beam distribution and resulting profile data as a function of the phase space orientation angle throughout the simulated scan

Simultaneous Algebraic Reconstruction

Each imaging ray interacts with a fractional pixel area “ a ”. Thus the following linear system describes each bin “ p_i ” in a projection, where “ f_j ” is each pixel’s value and “ w_{ij} ” is typically a non-square matrix of weighting factors based on how the imaging ray interacts with a pixel.

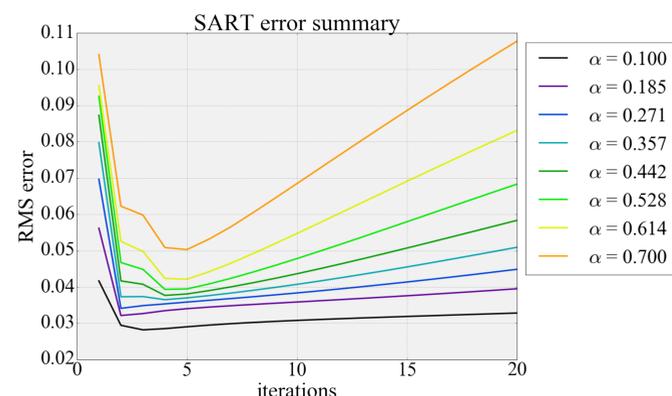
$$p_i = \sum_j w_{ij} f_j$$

SART is an iterative algorithm that solves this large and under-constrained linear system for “ f_j ” while comparing solutions to an initial “guess” and applying a correction for each iteration.



SART reconstruction of simulated beam transverse phase space

SART has two free parameters: the relaxation “ α ” and the number of iterations. Both must be fine-tuned to provide the best reconstruction with lowest artifacts and missing information, i.e. lowest RMS error.



SART reconstructions as a function of algorithm free parameters

References

- [1] A.C. Kak and M. Slaney. *Principles of Computerized Tomographic Imaging*. IEEE Press, 1988.
- [2] C.B. McKee, P.G. O’Shea, J. M. J. Madey, “Phase Space Tomography of Relativistic Beams”, Nucl. Instrum. Methods Phys. Res. A 358,264 (1995)
- [3] Scikit-image Python library: <http://scikit-image.org>